



Advances in live-cell single-particle tracking and dynamic super-resolution imaging

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Resolving the movement of individual molecules in living cells by single particle tracking methods has allowed many molecular behaviors to be deciphered over the past three decades. These methods have increasingly benefited from advances in microscopy of single nano-objects such as fluorescent dye molecules, proteins or nanoparticles as well as tiny absorbing metal nanoparticles. In parallel to these efforts aiming at tracking ever smaller and more photostable nano-objects in living cells, the development of localization-based super-resolution imaging provided means to increase the number of single molecules tracked on a single cell. In this review we will present the most recent advances in the field.

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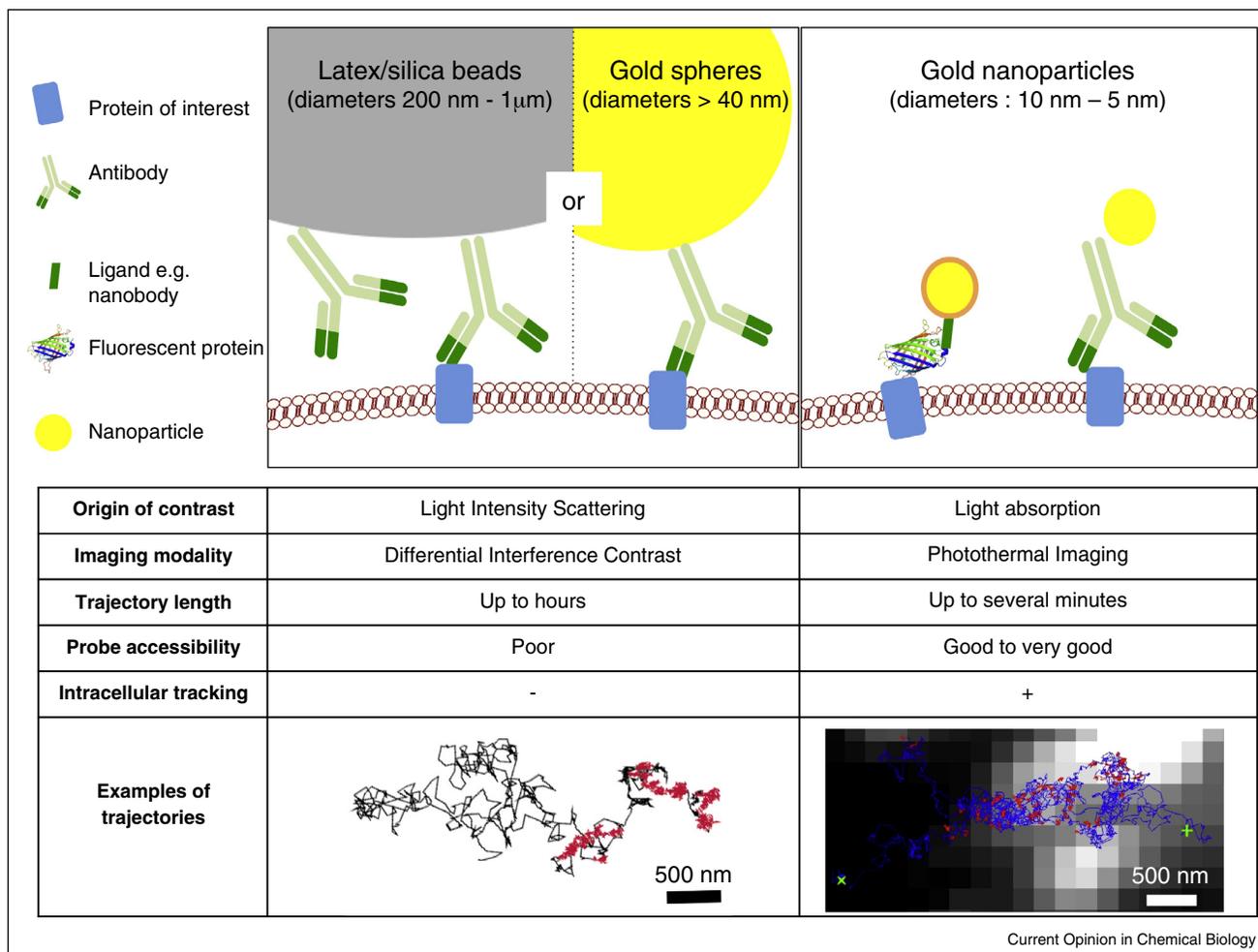
It is widely granted that understanding the complexity of cell functions requires deciphering the dynamic nature of constitutive molecule organizations. The movements of molecules in living cells are however characterized by their wide spatio-temporal diversities, making their study challenging. For instance, membranes exhibit an intrinsic complexity, because they consist of different lipids and a variety of proteins with dynamic and compartmentalized spatial distributions. Membrane molecules display various diffusion modes, frequently interact with each other at specific locations and can trigger signaling processes.

An important development in modern optical microscopy has been the detection of single molecules [1], in varied complex media including living cells [2–6]. Selecting a single molecule at a time allows the elimination of all the

implicit averages of conventional optical observations, gaining access to heterogeneity, dynamical fluctuations [7,8], diffusion [9], reorientation [10,11], colocalization, and conformational changes [12] at the molecular level. Single molecule microscopies have changed our approach for conceiving and carrying out experiments on complex molecular systems. Yet, the optical detection of a single molecule remains difficult, because its signal must be extracted from the background arising from billions of other molecules in the focal spot of a microscope. An elegant way to find the needle in the haystack is to attach a “label” to the molecule of interest. The ideal label must fulfill contradictory requirements. It should generate an intense optical signal, but at the same time be inert and as small as possible, not to perturb the observed molecule too severely. Finally, single molecule imaging and tracking provides the possibility to locate the molecule position with an accuracy well below the diffraction limit [13], the localization accuracy being mostly limited by the detection signal-to-noise ratio [14].

Several approaches have been used to track individual molecules mainly in the plasma membrane of live cells, with distinct advantages and limitations. The first reported method of Single Particle Tracking (SPT) uses non-fluorescent labels large enough to be detectable by conventional microscopes [15,16] through Rayleigh intensity scattering [17,18]. These labels can be large latex, polystyrene or silica particles of 200 nm to 1 μm diameter, or smaller metal particles [16] (Figure 1). When larger than typ. 40 nm, metal particles can indeed be imaged in optical microscopy by means of various methods, such as imaging at the plasmon frequency with dark field illumination [19], with differential interference contrast and video enhancement [18] or with total internal reflection [20]. SPT permits the tracking of individual molecules for very long times and possibly at very fast imaging rates [21]. SPT revealed for instance, barriers set for diffusion by the cytoskeleton [22], and the diversity of lateral diffusion modes of receptor for neurotransmitters in live neurons [23,24]. However, the size of the labels used in SPT precludes tracking single molecules in confined cellular regions [25*]. Indeed, Rayleigh scattering decreases like the sixth power of particle diameter [26] prohibiting the detection of particles smaller than 40 nm with conventional microscopy techniques mentioned above. This is particularly true if the particles are to be detected in cells or tissues where scattering signals must be discriminated from a strong background therein.

Figure 1



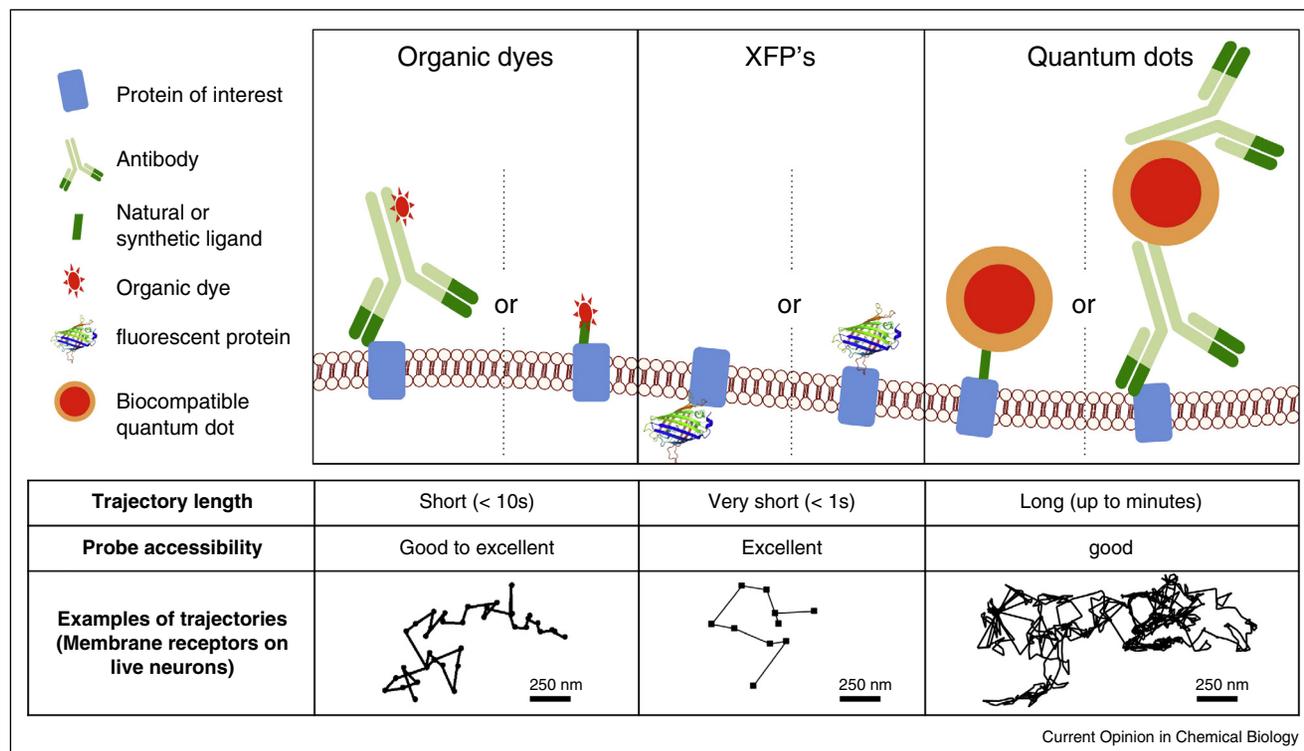
Principle and comparison of Single Particle Tracking techniques based on non-fluorescent probes. Examples of trajectories are adapted from [23] (left, gephyrin receptors tracked in the plasma membrane of live neurons) and correspond to integrins tracked inside labeled adhesion sites (white signal in background) of live cells (right). In both cases, red portions of the trajectories correspond to reduced diffusion transients of the tracked molecules.

An alternative approach for Single Molecule Tracking (SMT) is based on fluorescence (Figure 2). Single molecule fluorescence detection techniques arose in the 90s following the first demonstration at low temperature [27] and later on the first far-field detection at room temperature [28]. Indeed, by replacing scattering labels used in SPT by fluorescent molecules, SMT was demonstrated in synthetic membranes [29], then in living cells using organic dyes [2,3] or autofluorescent proteins [4]. Organic dyes can be chemically grafted to the molecule under study by several types of natural or synthetic ligands while autofluorescent proteins can be genetically fused to the protein of interest. Ligand-dye complexes can be so small as to neither hamper the diffusion of their host proteins or lipids, nor affect their functions or interactions with partners. The main drawback of fluorescence imaging is photobleaching, which severely limits the imaging times of single molecules. Removing free oxygen by

specific scavengers can reduce photobleaching, but this can be a serious obstacle to many experiments in living cells due to the toxicity of the oxygen scavengers. SMT is used to study many different systems in live cells, for instance membrane molecule dynamic organizations [2,30–35,36] or gene expression [37]. Recent noteworthy developments involve tracking single dye in 3D in cell membranes [38] and cell nuclei [39••].

Nanocrystals of semiconductors (quantum dots) have also been used as fluorescent markers [40,41]. They are more photostable than organic dyes and autofluorescent proteins. They however must be passivated, and functionalized by surface layers, because of their high chemical reactivity [42,43]. Functionalized quantum dots have proven to be extremely valuable tools for extended observation in living cells [44] and allow 3D single molecule tracking [45–47], for instance for the study of

Figure 2



Principle and comparison of Single Molecule Tracking techniques based on fluorescent probes. Examples of trajectories are adapted from [31] (left, glutamate receptors tracked in the plasma membrane of live neurons), from [98] (middle, glutamate receptor fused to a variant of YFP in live cell) and from [59] (right, AMPA receptor tracked in the plasma membrane of live neurons using antibody functionalized quantum dots).

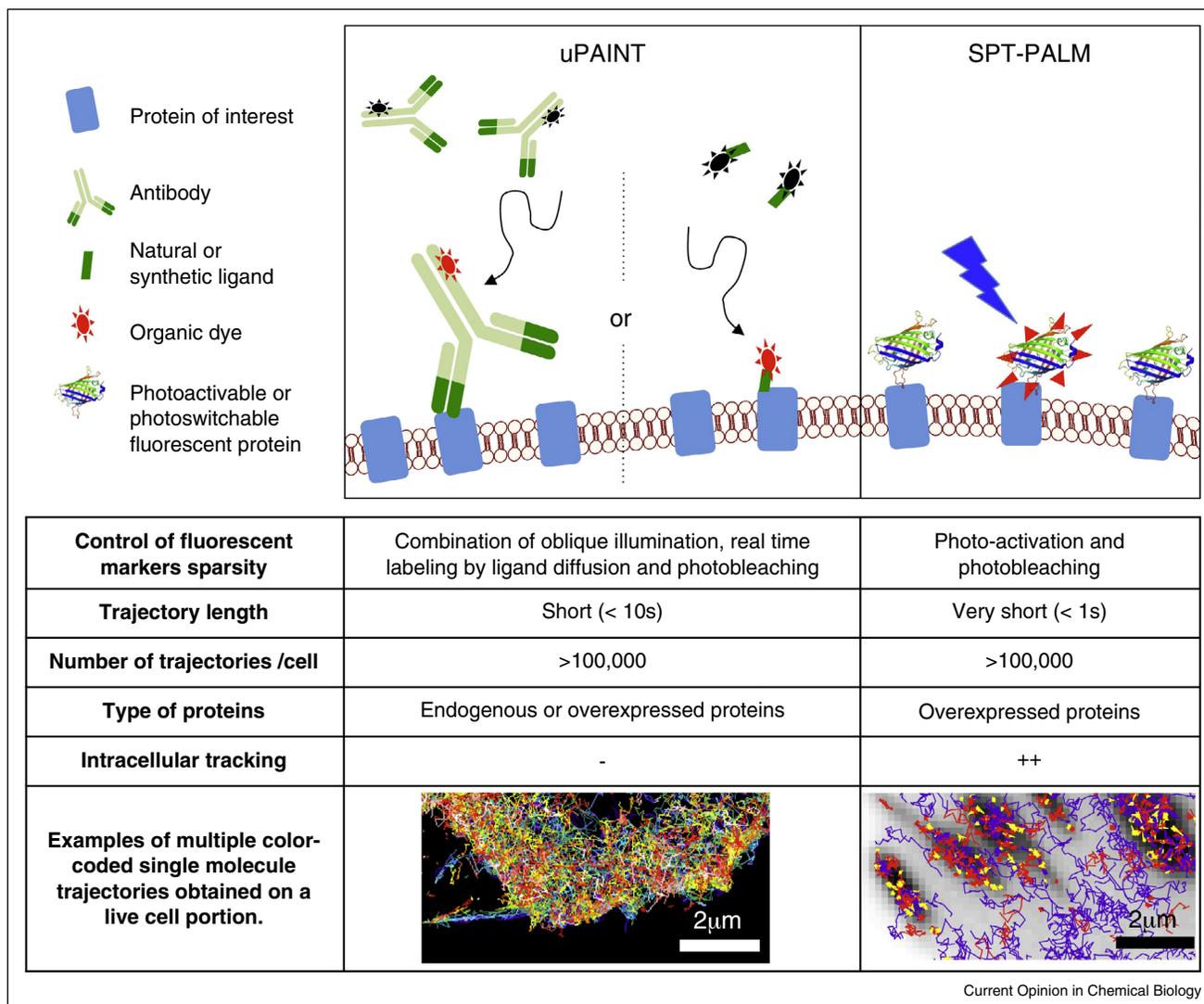
neurotransmitter receptors [48–51] in live neurons and transmembrane proteins in organotypic brain slices [52^{••}], of synaptic adhesion proteins [53] or of dimerization of epidermal growth factor receptors [54[•]]. However, quantum dot luminescence is subject to blinking [55] at all time scales [56] which renders observations of changes between different lateral diffusion modes of proteins challenging [57,58]. Moreover, once functionalized, quantum dot bulkiness may generate steric hindrance in confined cellular areas which may bias molecule diffusion like in synaptic clefts [59] or prevent access to adhesion sites [60[•]].

Single molecule methods, allowing the full history of proteins in cells including intermediate states even in highly confined regions to be recorded, would need to combine the advantages of SPT and SMT, namely long observation times and small nanometer-sized labels. An interesting approach consists in developing sensitive optical systems for the detection of the absorption of very small metal nanoparticles (NPs) [61]. Photothermal techniques have proven to be particularly valuable because the signal of NPs can be insensitive to the scattering environment of the cells [62,63]. Photothermal heterodyne imaging (PHI) [64] uses a combination of a time-modulated green beam to

heat the NPs and a non-resonant red beam to probe the local variations of the refraction index around the NPs [64,65]. In order to track single 5 nm gold nanoparticles a dedicated tracking strategy was developed [66]. It is based on triangulation acting like a nano-GPS, requiring only three local measurements around the nanoparticle of interest. This triangulation technique, which is able to reach a tracking rate of ~ 25 Hz is conceptually similar to that developed to track fluorescent beads in 3D by applying orbital movements of a confocal beam around a targeted bead [67]. To fully benefit from the small size of the perfectly photostable gold nanoparticles used in PHI, small and versatile absorbing probes have been developed for live cell imaging [60[•],68,69]. As an example, a probe consisting of a 5 nm gold NP functionalized with a GFP-nanobody, a small (2 nm \times 4 nm) fragment of camelidae antibody having a high affinity for GFP (Figure 1) allowed imaging and tracking in confined environments. Applications of PHI concern individual integrin tracking in adhesion sites [60[•]], NP internalization processes [70], intracellular tracking of microtubule end binding [60[•]] or FGF receptor tracking on the plasma of living cells [71] for instance.

Even if arbitrarily long time single-molecule tracking can be obtained with SPT techniques, the possibility to

Figure 3



Principle and comparison of localization based super-resolution techniques allowing high-density single molecule tracking. Examples are adapted from [83*] (left, activated EGF receptors tracked in the plasma membrane of live cells) and from [87*] (right, integrins tracked in and out adhesion sites of live cells).

simultaneously study a high number of individual molecules on a single cell is fundamentally limited by the diffraction limit which impose sparse labeling of single molecules to be resolved. Several algorithms have been developed to partially address this limitation [58,72–74]. Importantly, the recent developments of localization-based super-resolution methods opened new perspectives to study a high number of individual molecules on a single cell. Indeed, these methods deliver reconstructed images, which consist in a collection of single emitters localizations imaged successively at low density on a specimen of interest. This is either performed by iteratively activating a small number of photo-activable fluorophores among a dense population of inactivated ones

(such as in PALM [75,76], STORM [77] or related techniques [78,79]) or by real-time imaging stochastic molecular interactions (PAINT [80]) like fluorescent ligand binding to receptors (uPAINT [81*]). PALM and STORM inherently require photo-activable or photo-switchable fluorophores which can be either engineered fluorescent proteins (PALM) or emitters immersed in reducing agents to allow the photo-conversion (STORM) while uPAINT requires highly specific fluorescent ligands and is applicable to virtually any fluorophore detectable at the single molecule level. Because they are easily applicable to live cell studies, both uPAINT and the single particle tracking development of PALM (SPT-PALM [82**]) have become key

complimentary methods to allow single molecule tracking at high density (Figure 3). PALM benefits from the versatility of the fluorescent protein labeling toolbox including both intra and extra-cellular markers, while uPAINT, currently limited to extracellular binding on live cells, gives access to endogenous membrane receptors [81^{*}] and allows functional imaging of ligand activated receptors [83^{**}]. SPT-PALM and uPAINT were already applied in many different cellular systems such as neuronal membrane receptor organizations [84,85], adhesion sites [86,87^{*}], intracellular molecular organization of the cytoskeleton [88] or diffusive RNA binding proteins [89], RNA polymerase clustering [90^{*}] or EGF receptor dimerization states [83^{**}]. Interestingly, STORM was recently used for intracellular tracking of membrane receptors using SNAP-tags using live-cell compatible reducing agents [91^{*}]. A related approach to uPAINT uses small fluorescently labeled molecule agents that display reversible binding to sodium ion channel [92]. Interestingly, the specific super-resolution imaging and tracking of receptors dimers activated by their ligand in living cells [83^{**}] was recently

demonstrated combining single molecule FRET to dual-color uPAINT.

SPT and SMT have been very active fields of research over more than twenty years, delivering numerous key fundamental insights about the dynamic behavior of biomolecules in live cells. New developments are however still needed to track single molecules in highly confined and complex molecular environments both in live cells and tissues, either to obtain arbitrary long 3D trajectories or a ultra-high number of short trajectories in a small area. We foresee that further technical and conceptual developments in microscopy, chemistry, nanoscience or computer science, will continue to provide breakthroughs in biological science (Box 1).

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Box 1 Data analysis

Single particle/molecule positions are first to be identified in each image frame with nm accuracy using for instance centroid determination or Gaussian fitting of the particle optical signal as well as wavelet based algorithms [93]. Their 2D (or 3D) trajectories are then constructed using dedicated algorithms [57,58,73,94,95^{**}]. From the trajectories, the main method for analyzing molecule's modes of diffusion is to construct the mean square displacement (MSD) in order to calculate diffusion coefficient of single particles and further reveal the underlying modes of molecule diffusion mechanism [17]. For instance, a linear function of MSD versus time reveals random diffusion, while deviations from linearity can suggest active transport, confined diffusion, or other physical/chemical molecular interactions that impact diffusion modes. In addition to MSD analysis, which becomes prone to severe statistical imprecisions for short trajectories as often found in SMT, an analysis based on the distribution of the squared displacements has been shown to be particularly efficient [9,31,96]. The distribution of the squared displacements, $P(r^2, \tau)$ corresponds to the probability for molecule starting at the origin to be found within a circle of radius r after a time delay τ . From the shape of $P(r^2, \tau)$ over time delay, distinct diffusion modes corresponding to molecule subpopulations can be studied simultaneously [9,31,96].

Because with SPT-PALM and uPAINT the number of studied single molecule trajectories increased dramatically over conventional SMT approaches specific strategies were developed for data analysis, visualization and interpretation. For instance, in addition to MSD analysis and color-coded molecule trajectories displayed on a 2D image, (see Figure 3), 2D maps of the molecule mobilities are often produced [81^{*}]. These consist in displaying a color-coded image with each image pixel (whose size is chosen by the user, typically 200 nm) the median of the step lengths (corresponding to the distance between two consecutive points of a trajectory) found in this pixel. In addition, combining high-density single-molecule tracking and statistical inference, it was recently shown that it is possible to separately map the 2D diffusion and energy landscapes of membrane proteins across the cell surface at ~100 nm resolution [97].

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